

A 19-Channel d.c. SQUID Magnetometer System for Brain Research

J. FLOKSTRA, H. J. M. TER BRAKE, E. P. HOUWMAN, D. VELDHUIS, W. JASZCZUK, M. CASPARI and H. ROGALLA
University of Twente, Faculty of Applied Physics, P.O. Box 217, 7500 AE Enschede (The Netherlands)

A. MARTÍNEZ

Universidad de Zaragoza, E.T.S.I.I., Maria Zambrano 50, 50015 Zaragoza (Spain)

C. RILLO

I.C.M.A., C.S.I.C.-Universidad de Zaragoza, Servicio de Instrumentacion Cientifica, 50009 Zaragoza (Spain)

Abstract

A 19-channel d.c. SQUID magnetometer system for neuromagnetic investigations is under construction. The first-order gradiometers for sensing the signal are placed in a hexagonal configuration. D.c. SQUIDs based on niobium/aluminium technology have been developed, leading to a field sensitivity of about $5 \text{ fT}/\sqrt{\text{Hz}}$. SQUID read-out is realized with a resonant transformer circuit at 100 kHz. The multichannel control and detection electronics are compactly built.

1. Introduction

The superconducting quantum interference device (SQUID) is currently the most sensitive detector for measuring magnetic flux. SQUIDs are used in a large variety of applications of which neuromagnetism is the most remarkable [1]. The very weak fields originating from neural activity, being generally of the order of 10 to 1000 $\text{fT}/\sqrt{\text{Hz}}$ in the frequency range from d.c. up to about 100 Hz [2], can be detected by a SQUID sensor. The d.c. SQUID has an intrinsic flux sensitivity of about 10^{-5} to $10^{-6} \phi_0/\sqrt{\text{Hz}}$ (ϕ_0 is the flux quantum, $2.07 \times 10^{-15} \text{ Wb}$), leading to a field sensitivity below $10 \text{ fT}/\sqrt{\text{Hz}}$. The first magnetoencephalograms (MEG) were measured point by point, using the cryogenic equipment at a regular grid of measurement points around the head in order to map the brain

field distribution. For obtaining an acceptable signal-to-noise ratio, signal averaging has to be performed in many cases, so that in general only brain activity evoked by repeatable stimuli can be measured. This method is rather time consuming and often very inconvenient for the person under investigation. Further, it is not possible to measure adequately single brain events, like epilepsy. Nowadays, multichannel SQUID magnetometers have been developed by industrial and university groups in order to overcome the above-mentioned problems.

In this paper we describe several aspects of the development of a 19-channel d.c. SQUID magnetometer system that will be used in the μ -metal shielded room of the Biomagnetic Centre Twente. Attention will be paid to the d.c. SQUID sensor including the pick-up coil configuration (Section 2) and the multichannel electronics system (Section 3).

2. D.c. SQUID Sensor

The d.c. SQUID is in principle a superconducting loop interrupted by two Josephson junctions. The flux-voltage transfer function of the sensor is sinusoidal if an adequate bias current is applied and the sensitivity is of the order of $10\text{--}100 \mu\text{V}/\phi_0$ at the maximum slope. The SQUID is generally made in planar technology and flux is coupled to the SQUID ring by means of a planar multturn input coil on top of the washer-like configu-

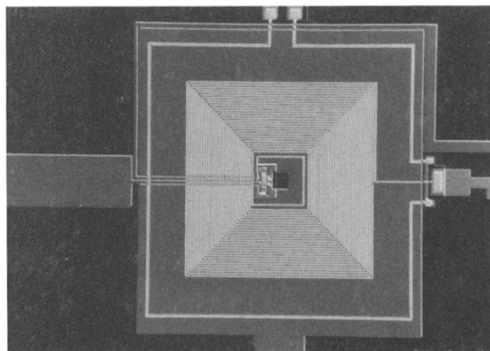


Fig. 1. Standard-type d.c. SQUID. The modulation coil (1 turn) and the input coil are on top of the washer. Typical outer dimensions 1 mm \times 1 mm.

ration. As an illustration one of our SQUIDS is shown in Fig. 1.

As a first step to SQUID fabrication, a reliable and well-controlled technique was developed for preparing high-quality Josephson tunnel junctions on the basis of niobium/aluminium technology [3]. Trilayers of Nb/Al, AlOx/Nb were prepared by d.c. magnetron sputter deposition, the aluminium oxide barrier being obtained by thermal oxidation of the aluminium at low oxygen pressure at room temperature. The junction areas of typically $5 \mu\text{m} \times 5 \mu\text{m}$ were defined by anodization of the trilayers protecting the junction area with photoresist. The junctions typically have gap voltages of 2.8–2.9 mV, critical currents of about 75% of the theoretical value and high sub-gap resistances leading to values of the quality parameter V_m of about 70 mV at 4.2 K and 1 V at 1.2 K. This demonstrates the high quality of our process.

Several SQUID configurations have been fabricated [4] using the technology developed for the Josephson junctions. The junctions are shunted by Pd resistances of about 3–5 Ω . The standard-configuration SQUIDS (Fig. 1) have been made with hole dimensions of $70 \mu\text{m} \times 70 \mu\text{m}$ and $145 \mu\text{m} \times 145 \mu\text{m}$. The junctions are placed at the inner side of the washer. The number of turns of the input coil is between 20 and 30. The peak-to-peak value of the flux-voltage transfer function is found to be about 30 μV being in agreement with our calculations. The flux

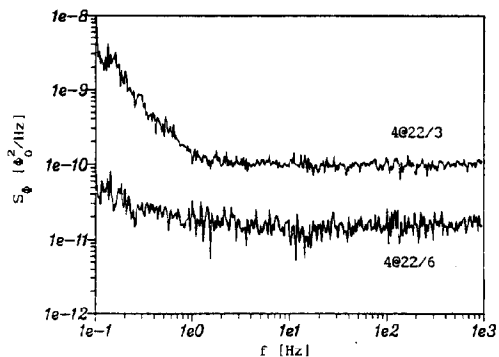


Fig. 2. Noise spectra of two standard d.c. SQUIDS. 4 @ 22/3: SQUID hole, $145 \mu\text{m} \times 145 \mu\text{m}$; equivalent field noise in sensing coil, 5 fT/ $\sqrt{\text{Hz}}$. 4 @ 22/6: SQUID hole, $70 \mu\text{m} \times 70 \mu\text{m}$; equivalent field noise in sensing coil, 3.5 fT/ $\sqrt{\text{Hz}}$.

noise according to theory is about $2 \times 10^{-6} \phi_0/\sqrt{\text{Hz}}$, but the experimental values are a factor of five to eight higher. This additional noise is most probably caused by resonances due to coupling between SQUID and input coil. The $1/f$ -noise corner point is about 1 Hz. Flux noise spectra for two of these SQUIDS are shown in Fig. 2.

Apart from the standard-type SQUID, resistively and inductively shunted SQUIDS were also fabricated. The SQUID hole is shunted by a resistance equal to the junction shunt resistance or an additional large-area loop, respectively. In these types of SQUIDS an input coil with a fixed inductance can be realized with a smaller number of turns as compared to the standard type, so that the deteriorating effect of the resonances can be diminished. The theoretical noise is about $1.5 \times 10^{-6} \phi_0/\sqrt{\text{Hz}}$, whereas the experimental values appeared to be only a factor of two to three higher.

The SQUID is connected to the pick-up coil section for sensing the magnetic fields. The pick-up coils consist of wire-wound first-order gradiometers having two sections of three turns with a diameter of 20 mm and a base line length of 40 mm [5]. The distance between the turns of the lower sensing section is 0.5 mm, whereas that of the turns of the compensating section is 6 mm. The self inductance of the pick-up coil is 0.8 μH and that of the input coil of the SQUID about 0.1 μH .

Our magnetometer has 19 channels placed in a hexagonal configuration somewhat tilted with respect to each other (9.5 degrees) in order to fit to the concavely shaped bottom of the tail of the cryostat. In addition, three channels are available for measuring the orthogonal field components in order to compensate the imbalance effects of the gradiometers. Furthermore two channels are present to measure two spatial derivatives for further noise rejection. The flux transformer circuits in a multichannel system may easily invoke crosstalk and in order to eliminate this, external feedback to the flux transformer is applied [6].

The SQUID chip is placed in a rigid, compartmentalized Nb module. The module, consisting of several shielded sections, also contains the feedback inductor and the resonating circuit for the SQUID read-out.

3. Electronics

The read-out of the SQUID is realized by using this periodic flux-voltage converter in a flux-locked loop. A modulation signal with a frequency of 100 kHz and an amplitude equivalent to $\phi_0/4$ is applied to the SQUID

for biasing at maximum sensitivity. Feedback from the output of the detection electronics to the SQUID gives the linearization of the magnetometer in the frequency range of interest (< 1 kHz).

The block diagram of a single channel of the electronics system is shown in Fig. 3. The dashed box contains all channel elements placed inside the cryostat. The preamplifiers are inside an r.f. shielded aluminium box internally compartmentalized and placed on top of the cryostat. The other elements of the Figure are outside the magnetically shielded room in a separate r.f. shielded cabinet.

The preamplifier consists of U311 FETs in a cascode configuration, loaded with an *RLC* network resonating at the modulation frequency of 100 kHz. The preamplifier voltage noise E_n is about $1 \text{ nV}/\sqrt{\text{Hz}}$ at this frequency. The quality factor is about five, thus giving a bandwidth of 20 kHz. The gain is about 50, being enough to make the noise contributions of the following stages negligible compared to the preamplifier noise.

A small resonant transformer is used between the SQUID and the preamplifier in order to reduce the effect of the preamplifier noise with respect to the SQUID noise. The forward transfer ratio of the SQUID is

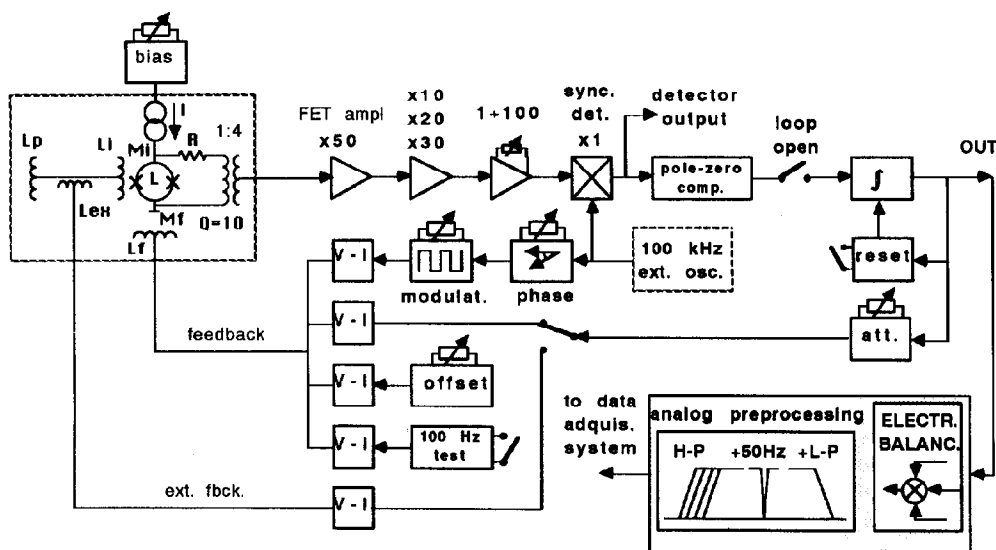


Fig. 3. D.c. SQUID control and detection electronics and analog preprocessing.

roughly $70 \mu\text{V}/\phi_0$ so that a minimum gain of about 20 is needed for the resonant transformer in order to limit the electronic noise contribution to about $10^{-6} \phi_0/\sqrt{\text{Hz}}$. The current noise I_n , being about $40 \text{ fA}/\sqrt{\text{Hz}}$, is dominated by the impedance of the transfer line between the preamplifier and resonant transformer, and it gives a negligible contribution to the total noise. The selected gain for the transformer is 40. A moderate Q -factor of 10 was chosen to give a bandwidth of 10 kHz, so that the voltage gain of the transformer should be about four. A prototype transformer has been made of 0.1 mm Cu wire. It is a cylindrical coil former with a length of 5 mm and an outer diameter of 5.8 mm, thus fitting in the 7 mm hole of the SQUID module. The prototype consisted of 90 primary and 635 secondary turns. The measured inductances are $17.4 \mu\text{H}$ ($27.5 \mu\text{H}$) and $490 \mu\text{H}$ ($760 \mu\text{H}$) respectively, whereas the coupling factor appeared to be 0.81 (0.89) (transformer voltage gain 4.3 (4.7)). The values between brackets were measured outside the superconducting enclosure. The series resistances of the coils are below 1Ω so that the noise contribution can be neglected. The transformer is brought into resonance at the modulation frequency of 100 kHz with a shunt capacitor connected at the secondary side and placed inside the SQUID module.

The detector/controller electronics are realized in a miniaturized version on a single Eurocard for each channel. Because of the miniaturization and the fact that the system is not designed to be a general purpose magnetometer, several parameters have been fixed, including the sensitivity and the frequency bandwidth (5 kHz). The sensitivity is 1 V at the output for $1 \phi_0$ in the SQUID. The full scale of 10 V corresponds to an effective field of about 3 nT in the gradiometer. The expected dynamic range in a 100 Hz measurement bandwidth is 2.5×10^5 . Both a step-gain and a variable-gain amplifier for adjusting the open-loop gain are placed between the preamplifier and the phase-sensitive detector. An external oscillator provides the modulation signal for all channels. The flux modula-

tion phase and peak-to-peak amplitude are set by potentiometers in the detector/controller unit.

The open-loop transfer function has a low-frequency pole of the integrator, and two high-frequency poles due to the resonant transformer (5 kHz) and the RLC load of the preamplifier (10 kHz). Furthermore, a lag-lead pole-zero compensation circuit has been added for dynamic behaviour optimization [7]. The slew rate is $7500 \phi_0/\text{s}$ after compensation.

The electronics have been developed independently from the d.c. SQUID devices. System parameters such as dynamic behaviour, the gain of the feedback path and the open-loop gain have been adjusted by means of a d.c. SQUID simulator [8].

Other modules included in the electronics are a manual/automatic reset, an offset for zero adjustment, and a 100 Hz saw-tooth generator for optimum bias current, modulation amplitude and phase-shift settings. A switch selects between internal or external feedback. The sensitivity is adjusted with an attenuator in the feedback path.

Before the A/D conversion the signal is first processed with the electronic balancing module [9] and then some analog filtering is necessary. For this purpose we developed a 50 Hz adaptive notch filter that suppresses the mains frequency by more than 60 dB with a bandwidth of only 1 Hz. Further, high-pass and low-pass filters will be applied, the latter also functioning as anti-alias filters for the 1 kHz sampling frequency. Thus signals can be measured without significant phase shift up to a frequency of 100 Hz, which is adequate for most biomagnetic experiments.

4. Conclusions

A 19-channel d.c. SQUID magnetometer is under construction. A reliable and well-controlled technique for the fabrication of SQUID sensors based on Nb and Al has been developed. SQUIDs with a noise level between 5×10^{-6} and $10^{-5} \phi_0/\sqrt{\text{Hz}}$ have been

fabricated so that magnetic fields below $10 \text{ fT}/\sqrt{\text{Hz}}$ can be measured. Miniaturized multichannel control and detection electronics have been developed.

References

- 1 J. Clarke, SQUIDS, brains and gravity waves, *Phys. Today*, (1986) 36–44.
- 2 G. L. Romani, Biomagnetism: An application of SQUID sensors to medicine and physiology, *Physica B*, 126 (1984) 70–81.
- 3 E. P. Houwman, D. Veldhuis, J. Flokstra and H. Rogalla, Fabrication and properties of Nb/Al, AlOx/Nb Josephson tunnel junctions with a double oxide barrier, *J. Appl. Phys.*, 67 (1990) 1992–1994.
- 4 E. P. Houwman, D. Veldhuis, J. Flokstra and H. Rogalla, Comparison of shunted DC-SQUIDS with large β , *Physica B*, 165/166 (1990) 81–82.
- 5 H. J. M. ter Brake, J. Flokstra, E. P. Houwman, D. Veldhuis, W. Jaszczuk, A. Martinez and H. Rogalla, Design and construction of a 19-channel DC-SQUID neuromagnetometer, *Physica B*, 165/166 (1990) 95–96.
- 6 H. J. M. ter Brake, F. M. Fleuren, J. A. Ulfman and J. Flokstra, Elimination of flux-transformer crosstalk in multichannel SQUID magnetometers, *Cryogenics*, 26 (1986) 667–670.
- 7 C. Rillo, D. Veldhuis and J. Flokstra, Optimization of the dynamic behavior of a SQUID system using an electronic simulation, *IEEE Trans. Instrum. Meas.*, IM-36 (1987) 770–775.
- 8 A. Martinez, J. Flokstra, C. Rillo, L. A. Angurel, L. M. Garcia and H. J. M. ter Brake, Low noise SQUID simulator with large dynamic range of up to eight flux quanta, *Cryogenics*, 30 (1990) 324–329.
- 9 H. J. M. ter Brake, Z. Dunajski, W. A. G. van der Mheen and J. Flokstra, Electronic balancing of multichannel SQUID magnetometers, *J. Phys. E: Sci. Instrum.*, 22 (1989) 560–564.